Is synchronised NIPPV more effective than NIPPV and NCPAP in treating apnoea of prematurity (AOP)? A randomised cross-over trial

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ABSTRACT

Background Apnoea, desaturations and bradycardias are common problems in preterm infants which can be treated with nasal continuous positive airway pressure (NCPAP) and nasal intermittent positive pressure ventilation (NIPPV). It is unclear whether synchronised NIPPV (SNIPPV) would be even more effective.

Objective To assess the effects of flow-SNIPPV, NIPPV and NCPAP on the rate of desaturations and bradycardias in preterm infants and, secondarily, to evaluate their influence on pattern of breathing and gas exchange.

Patients and methods Nineteen infants (mean gestational age at study 30 weeks, 9 boys) with apneic spells were enrolled in a randomised controlled trial with a cross-over design. They received flow-SNIPPV, NIPPV and NCPAP for 4 h each. All modes were provided by a nasal conventional ventilator able to provide synchronisation by a pneumotachograph. The primary outcome was the event rate of desaturations (≤80% arterial oxygen saturation) and bradycardias (≤80 bpm) per hour, obtained from cardiorespiratory recordings. The incidence of central apnoeas (≥10 s) as well as baseline heart rate, FiO2, Spo2, transcutaneous blood gases and respiratory rate were also evaluated.

Results The median event rate per hour during flow-SNIPPV, NIPPV and NCPAP was 2.9, 6.1 and 5.9, respectively (p=0.001 and 0.009, compared with flow-SNIPPV). Central apnoeas per hour were 2.4, 6.3 and 5.4, respectively (p=0.001, for both compared with flow-SNIPPV), while no differences in any other parameter studied were recorded.

Conclusions Flow-SNIPPV seems more effective than NIPPV and NCPAP in reducing the incidence of desaturations, bradycardias and central apnoea episodes in preterm infants.

INTRODUCTION

Apnoea of prematurity (AOP) is a common problem in preterm infants. Desaturations and bradycardias, considered as mainly elicited by AOP, are associated with longer-term neurodevelopmental problems.1–4 Standard therapies to treat these conditions are nasal continuous positive airway pressure (NCPAP) and methylxanthines. For infants who do not respond to this combined strategy, nasal intermittent positive pressure ventilation (NIPPV) has been proposed as an alternative to NCPAP.5–7 as it may provide a greater respiratory support. It is unclear whether synchronised NIPPV (SNIPPV) would be even more effective, as synchronisation may add some favourable effects. Our aim was thus to compare the effects of flow-SNIPPV, NIPPV and NCPAP on the rate of desaturation events and bradycardias in preterm infants and, secondarily, to evaluate their influence on pattern of breathing and gas exchange. Our hypothesis was that flow-SNIPPV is more effective than NIPPV and NCPAP.

METHODS

Patients

Between October 2010 and February 2012, newborn infants admitted to the neonatal intensive care unit (NICU) at “S. Giovanni Calibita” Fatebenefratelli Hospital of Rome were screened for eligibility. Inclusion criteria were: (1) gestational age <34 weeks by maternal dates or early ultrasound, (2) postmenstrual age at time of study ≤38 weeks, (3) requirement for NCPAP to treat AOP and (4) fraction of inspired oxygen (FiO2) need ≤0.3. At the time of the study, all infants were receiving caffeine citrate (5 mg/kg/day) and were in stable conditions except for their apnoeic episodes.
Infants with congenital or chromosomal abnormalities, acute infections, anaemia, electrolyte imbalances, intraventricular haemorrhage or patent ductus arteriosus were excluded. Written informed parental consent was obtained for each infant.

Study design and protocol
A randomised cross-over study with three treatment phases was conducted. Following recruitment, infants were randomly allocated to the six possible sequences of flow-SNIPPV, NIPPV and NCPAP applied for 4 h each. Four patients were allocated to sequence NIPPV/NCPAP/SNIPPV while three patients were allocated to each of the remaining five sequences.

The sequence to be followed in each patient was revealed to the investigators immediately before recording by a telephone call. Throughout the study, infants were fed at 3 h intervals and received their routine care while in an incubator at thermoneutrality and in a supine position. The study protocol was approved by the Ethics Committee of the hospital.

Respiratory support system
Flow-SNIPPV, NIPPV and NCPAP were applied using ‘Giulia’ neonatal ventilator via nasal prongs (Ginevri Medical Technologies, Rome, Italy). Synchronisation was obtained by means of a fixed orifice pneumotachograph (2.5 mm inner diameter—dead space 1 mL) interposed between the prongs and the Y piece. The largest possible prongs were used, with a snug fit to avoid leakage. No precautions were taken to avoid leakage from the mouth. For all ventilation modes initial flow was set at 8 L/min and FiO2 adjusted to keep pulse oximeter saturation (SpO2) between 90% and 94%. The system was regularly monitored and flow delivered by the ventilator adjusted in order to keep positive end-expiratory pressure constant on selected values. Flow-SNIPPV was delivered in the assist/control mode (ie, the ventilator assisted each spontaneous breath) with the following parameters: Ti 0.3–0.35 s, peak inspiratory pressure (PIP) 15 cm H2O, positive end-expiratory pressure 5–6 cm H2O and back-up rate 20 bpm. Trigger level was initially set at 0.1 L/min, then adjusted for each infant in order to obtain the best synchronisation and avoid autotriggering. Synchronisation was continuously monitored during SNIPPV by one of the authors who attended the registration, looking at the ventilator’s and the infant’s spontaneous respiratory rate (RR). In order to facilitate the detection of synchrony, synchronous breaths are displayed on the ventilator’s screen as a bicolour pressure trace, green for inspiration and white for expiration, while mandatory mechanical breaths are displayed as a white pressure trace during inspiration and expiration. To avoid autotriggering and low signal detection, the nose of the infants, the flow sensor and the ventilator circuit were regularly inspected and kept clear of secretion and humidity. NIPPV was delivered using the same parameters as flow-SNIPPV at a mechanical RR of 20 bpm. During flow-SNIPPV and NIPPV, peak pressure could be increased up to max 20 cm H2O to obtain effective euation per auscultation and according to blood gases. NCPAP was set at 5–6 cm H2O.

Cardiorespiratory recordings
Throughout the study the following signals were monitored and recorded (Infinity Delta XL Monitor and GateWay Plus computerised polygraphic system, Dräger Medical System, Lübeck, Germany): thoracic impedance and RR, pulse oximetry waveform and SpO2, ECG waveform and beat-to-beat heart rate (HR), transcutaneous O2 and CO2 pressures (PtCO2 and PtcCO2), RR, SpO2, HR and transcutaneous blood gases were in 2 s averaging mode. Airway pressure, airway flow and FiO2 from ‘Giulia’ Ventilator were also recorded. Sensors applied to infants and their output signals were regularly checked during recordings. Physiological signals were simultaneously recorded on a computer (Compaq 6720s, Hewlett-Packard, Palo Alto, California, USA) and afterwards imported on specific software developed on the MATLAB platform, to be analysed off-line. To improve the detection of central apnoeas, the thoracic impedance signal was low-pass filtered to remove the contribution of the cardiac signal that might be mistaken for breathing. The cut-off frequency of low-pass filter was obtained by fast Fourier transform of the thoracic impedance signal and set according to the highest RR appearing during the whole monitored time for each infant. Recordings were analysed without access to clinical data. A desaturation was defined as a fall in SpO2 to ≤80% for >1 s and a bradycardia as a fall in HR to ≤80 bpm for more than one beat. Desaturations and bradycardias associated with a distorted signal immediately prior to their onset were excluded. A central apnoea was scored if the filtered thoracic impedance signal showed an absence of spontaneous chest wall movement due to breathing for ≥10 s. Simultaneous thoracic impedance and ECG signals were analysed on the occasion of each bradycardia to exclude cardiac artefacts on apnoea detection. Desaturations and bradycardias were considered as temporally related to an apnoeic spell if their onset occurred within 15 s from the onset of a central apnoea. Mixed and obstructive apnoeas were not analysed. Baseline RR, HR, SpO2, tcPO2 and tcPCO2 were defined as the mean of the respective parameter within artefact-free recording time and calculated using a MATLAB based software. Finally, event rates for desaturations, bradycardias and central apnoeas were calculated as the number of respective events per hour of artefact-free recording time.

Statistical methods
Sample size calculation was based on a preliminary analysis including six patients treated with NCPAP that showed a mean (SD) of 5.5 (1.8) desaturation and/or bradycardia events per hour, considered as our primary outcome. As NIPPV seems to offer no advantages over NCPAP to treat apnoea, we hypothesised that flow-SNIPPV could reduce these adverse events by 40%. Assuming a common SD for all modes of ventilation, 19 participants were considered sufficient to detect a significant reduction of 40% (from 5.5 to 3.6 desaturation and/or bradycardia events per hour) using flow-SNIPPV compared with NIPPV and NCPAP, considering 0.05 type I and 0.2 type II errors and taking into account multiple comparisons.

Descriptive statistics as numbers and percentages as well as median and IQR were used to summarise demographic and clinical characteristics of the enrolled infants. Sequence, carryover

Table 1  Demographic and clinical characteristic of enrolled infants (n=19)

<table>
<thead>
<tr>
<th>Characteristic</th>
<th>Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Birth weight (g)</td>
<td>800 (678–1068)</td>
</tr>
<tr>
<td>Gestational age at birth (weeks)</td>
<td>27 (25–28)</td>
</tr>
<tr>
<td>Boys</td>
<td>9 (47)</td>
</tr>
<tr>
<td>Body weight* (g)</td>
<td>986 (722–1168)</td>
</tr>
<tr>
<td>Postmenstrual age* (weeks)</td>
<td>30 (29–31)</td>
</tr>
<tr>
<td>FiO2*</td>
<td>0.21 (0.21–0.26)</td>
</tr>
<tr>
<td>Haematocrit* (%)</td>
<td>36 (32–40)</td>
</tr>
<tr>
<td>Days on caffeine*</td>
<td>20 (13–29)</td>
</tr>
<tr>
<td>Milk intake* (mL/kg)</td>
<td>96 (68–137)</td>
</tr>
</tbody>
</table>

Data are expressed as median (IQR) and number (%) .
*At time of study.
and period effects were analysed using a linear mixed model. Due to the small sample size and the repeated measures in the same patient, a non-parametric Friedman’s test was used for comparisons between treatment modes. A post hoc analysis was done using Bonferroni adjustment if a global test revealed significant differences. A p value <0.05 was considered statistically significant. All analyses were carried out with STATA V.12.1.

RESULTS

Within the study period, 24 infants met the inclusion criteria, but only 19 parents gave consent. Demographic and clinical characteristics of enrolled infants are presented in table 1. Sixteen (84.2%) of them were treated with invasive mechanical ventilation for respiratory distress. In these infants intubation lasted mean (SD) 9.4 (11.3) days and they were studied at mean (SD) 12.8 (5.7) days after extubation. All infants received surfactant, three of them by means of the INSURE approach. All patients were on NCPAP at the time of study. Nine (47.4%) infants were still on oxygen at enrolment.

As regards the primary study outcome, the median rate of desaturation events and/or bradycardias per hour during flow-SNIPPV was significantly lower than during NIPPV (2.9 vs 6.1, p=0.009) and NCPAP (2.9 vs 5.9, p<0.001) (table 2). No significant effect was found for sequence (p=0.499), carryover (p=0.451) and period (p=0.271). After adjusting, mean differences from SNIPPV were 3.10 (95% CI 1.5 to 4.7) for NIPPV and 2.74 (95% CI 1.2 to 4.3) for NCPAP. The fraction of desaturations occurring in association with central apnoeas were mean (SD) 0.46 (0.36) during SNIPPV, 0.55 (0.34) during NIPPV and 0.51 (0.33) during NCPAP (p=0.183). Four (21%) infants showed no bradycardias during the whole registration period. Of all the recorded bradycardias, mean (SD) 82.3 (15.6)% were related to an apnoeic spell.

Regarding the secondary study variables (table 3), a decrease in central apnoeas per hour was observed during flow-SNIPPV compared with NIPPV (2.4 vs 5.3, p=0.001) and NCPAP (2.4 vs 6.3, p=0.001). No significant effect was found for sequence (p=0.529), carryover (p=0.111) and period (p=0.806). Baseline cardiorespiratory parameters were significantly different during the three modes of non-invasive ventilation (NIV) according to the Friedman test, but these differences were lost after Bonferroni adjustment. The duration of the hypoxic events and bradycardias was not influenced by the mode of ventilation. No severe adverse events were reported during the study. Figures 1–5 illustrate typical traces of airway pressure, flow and thoracic impedance recorded throughout the study. In most infants, flow-SNIPPV and NIPPV backup pressure peaks produced no chest inflations during apnoea.

DISCUSSION

While NCPAP is considered effective in treating AOP, studies on NIPPV reported conflicting results.5–7 Recently Pantalitschka,8 observed that variable-flow NCPAP and NIPPV were more effective than conventional ventilator NIPPV in improving symptoms related to AOP, and encouraged further studies to investigate how SNIPPV performs. According to our results, flow-SNIPPV therapy was associated with an overall reduction in the combined incidence of adverse events, desaturations and bradycardias, by about 40% when compared with NIPPV and NCPAP, and also resulted in a 50% decrease in the incidence of central apnoeas. The fraction of desaturations occurring in association with central apnoeas was similar during all modes of ventilation. No statistically significant differences were observed in the measured cardiorespiratory parameters on post hoc testing of paired groups.

Table 2 Desaturation (≤80%) and bradycardia (≤80 bpm) events per hour of artefact-free recording time (n=19)

<table>
<thead>
<tr>
<th>Mode of ventilation</th>
<th>SNIPPV</th>
<th>NIPPV</th>
<th>NCPAP</th>
<th>p Value*</th>
<th>SNIPPV (p)† vs NIPPV</th>
<th>vs NCPAP</th>
</tr>
</thead>
<tbody>
<tr>
<td>Desaturations and/or bradycardias</td>
<td>2.9 (0.75–6.8)</td>
<td>6.1 (3.1–9.4)</td>
<td>5.9 (2–10.3)</td>
<td>&lt;0.001</td>
<td>0.009</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Desaturations ≤80%</td>
<td>2.9 (0.5–7.2)</td>
<td>6.1 (2.9–9.4)</td>
<td>5 (1.2–10.1)</td>
<td>&lt;0.001</td>
<td>0.059</td>
<td>0.046</td>
</tr>
<tr>
<td>Bradycardias ≤80 bpm</td>
<td>0 (0–0.48)</td>
<td>0 (0–0.52)</td>
<td>0.24 (0–1.4)</td>
<td>0.025</td>
<td>1.000</td>
<td>0.195</td>
</tr>
</tbody>
</table>

*Data are expressed as median (IQR).
†Friedman’s test.
NCPAP, nasal continuous positive airway pressure; NIPPV, nasal intermittent positive pressure ventilation; SNIPPV, synchronised NIPPV.

Table 3 Secondary study variables (n=19)

<table>
<thead>
<tr>
<th>Mode of ventilation</th>
<th>SNIPPV</th>
<th>NIPPV</th>
<th>NCPAP</th>
<th>p Value*</th>
<th>SNIPPV (p)† vs NIPPV</th>
<th>vs NCPAP</th>
</tr>
</thead>
<tbody>
<tr>
<td>Central apnoeas (≥10 s) per hour</td>
<td>2.4 (1–3.6)</td>
<td>6.3 (2.8–17)</td>
<td>5.4 (3.1–12)</td>
<td>0.002</td>
<td>0.001</td>
<td>0.001</td>
</tr>
<tr>
<td>HR (bpm)</td>
<td>156 (150–161)</td>
<td>158 (149–162)</td>
<td>159 (154–163)</td>
<td>&lt;0.001</td>
<td>0.481</td>
<td>0.111</td>
</tr>
<tr>
<td>Baseline RR (bpm)</td>
<td>57 (50–64)</td>
<td>54 (49–60)</td>
<td>53 (47–57)</td>
<td>0.058</td>
<td>0.440</td>
<td>0.663</td>
</tr>
<tr>
<td>FiO₂</td>
<td>0.22 (0.21–0.25)</td>
<td>0.21 (0.21–0.26)</td>
<td>0.22 (0.21–0.26)</td>
<td>0.000</td>
<td>0.607</td>
<td>0.814</td>
</tr>
<tr>
<td>SpO₂ (%)</td>
<td>91 (90–96)</td>
<td>91 (90–93)</td>
<td>91 (90–97)</td>
<td>0.003</td>
<td>0.061</td>
<td>0.185</td>
</tr>
<tr>
<td>PtcO₂ (mm Hg)</td>
<td>58 (45–71)</td>
<td>54 (49–75)</td>
<td>53 (48–68)</td>
<td>0.020</td>
<td>1.887</td>
<td>1.015</td>
</tr>
<tr>
<td>PtcCO₂ (mm Hg)</td>
<td>49 (46–52)</td>
<td>52 (43–58)</td>
<td>49 (42–55)</td>
<td>0.018</td>
<td>1.849</td>
<td>0.787</td>
</tr>
</tbody>
</table>

*Data are expressed as median (IQR).
†Friedman’s test.
HR, heart rate; NCPAP, nasal continuous positive airway pressure; NIPPV, nasal intermittent positive pressure ventilation; RR, respiratory rate; SNIPPV, synchronised NIPPV.
Although promising, these results should be interpreted with due caution. First, only a small number of infants was included, even though the sample size required to show statistically significant differences in the outcome data consisted of 19 infants. Furthermore, extremely low birthweight infants, that are particularly prone to adverse events, were highly represented in our population as 12 infants weighed <1000 g at birth, and 9 at the time of recording. Second, the study cross-over periods were 4 h long, and no information on longer-term outcome can be provided.

According to our results, the efficacy of flow-SNIPPV was mostly due to a decrease in desaturation events, as the rate of bradycardias per hour was quite low among enrolled infants. We speculate that flow-SNIPPV limited oxygenation instability either by reducing the incidence of adverse events related to AOP as well as through different effects on ventilation. Preterm infants are particularly prone to loss of functional residual capacity (FRC) due to the excessive chest wall compliance, while the softness of the upper airway tissues may predispose to obstruction. Several studies showed that increasing NCPAP levels reduce the frequency of central apnoeas and periodic breathing.\textsuperscript{10–12} Nevertheless, high pressures in infants with minimal lung disease may decrease cardiac output,\textsuperscript{13–15} and increase the risk of pneumothorax.\textsuperscript{16} Alternatively, mean airway pressure (MAP) can be increased by increasing mechanical RR during NIPPV or by using SNIPPV. The latter, however, seems to be a more logical solution as synchronous

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Figure 1  Time tracing of delivered pressure, air flow and thoracic impedance (unfiltered (light gray) and filtered (dark gray)) showing the typical pattern recorded during an apnoeic episode while on flow-synchronised nasal intermittent positive pressure ventilation. In all traces inspiration is up. Mechanical breaths follow infant’s spontaneous ones before and after the respiratory pause. No chest inflation is detected during the apnoeic spell despite mechanical backup breaths.

Figure 2  Time tracing of delivered pressure, air flow and thoracic impedance (unfiltered (light gray) and filtered (dark gray)) showing the typical pattern recorded during an apnoeic episode while on nasal intermittent positive pressure ventilation. In all traces inspiration is up. During the apnoeic spell, backup mechanical breaths did not result in any chest inflation.
mechanical breaths, delivered when the glottis is open, may be more effectively transmitted to the lungs, improving ventilation. Conversely, asynchronous breaths may induce laryngeal closure and inhibit inspiration, increase abdominal distension, cause volutrauma and pneumothorax, have detrimental effects on blood pressure and cerebral blood flow, and increase work of breathing (WOB). Contrariwise, a reduced WOB improves hypoxaemic episodes and apnoea, and SNIPPV decreases WOB compared with NCPAP and NIPPV.

Technical issues also determine the effectiveness of synchronisation and may be responsible for our findings. Until present, two devices have been commonly used to trigger the ventilator during NIV in preterm infants: the abdominal capsule, and the flow sensor. Recently, a device using a diaphragmatic electromyogram has been introduced, however little data are available on clinical outcomes. The abdominal capsule, although quite effective, has some disadvantages relating to the high sensitivity to the infant’s spontaneous movements and to the considerable skill required for correct placement. Studies reporting on abdominal capsule-SNIPPV for AOP as secondary outcome showed contrasting findings. Conversely, airway flow detection is a recognised and easy means for synchronising. Moreover, it offers an advantage when preterm infants employ breathing strategies with inversion of the usual sequence, that is, diaphragmatic contraction commences in advance of glottic opening, occurring in up to 60% of spontaneous breaths.

Figure 3  Time tracing of delivered pressure, air flow and thoracic impedance (unfiltered (light gray) and filtered (dark gray)) showing the typical pattern recorded while on flow-synchronised nasal intermittent positive pressure ventilation. In all traces inspiration is up. Mechanical breaths follow infant’s spontaneous ones.

Figure 4  Time tracing of delivered pressure, air flow and thoracic impedance (unfiltered (light gray) and filtered (dark gray)) showing the typical pattern recorded while on nasal intermittent positive pressure ventilation (NIPPV). In all traces inspiration is up. NIPPV breaths occur at different stages of the spontaneous respiratory cycle ((1) peak of breath, (2) mid-expiration, (3) late expiration, (4) peak of breath, (5) early expiration, (6) mid-expiration). Infant seems not to be entrained with the ventilator.
A common criticism of using a flow sensor for NIV is that its reliability can be altered by the continuous flow passing through it, generated by the variable leaks from the infant’s nostrils and mouth. To obtain synchronisation, the study ventilator’s software elaborates the flow signal detected by the pneumotach. The steady component of flow generated by the continuous variable leaks is quantified and deducted, while the fast variations of flow due to spontaneous breathing are used to trigger the ventilator. The reliability of the system has been tested in a simulated neonatal model, showing that its performance is not affected by the leaks.37

A technical limitation possibly affecting our results is that cardiac artefacts may impair the standard impedance pneumography in the detection of central apnoeas.8 However, we improved the accuracy of the technique by devising a new filtering strategy, afterwards confirmed by Lee.38 Moreover, we were not able to analyse mixed and obstructive apnoeas, due to the concurrent presence of respiratory movements from infants and flow signal from mechanical breaths during flow-SNIPPV and NIPPV. Nevertheless, the distinction between central and mixed/obstructive spells should not be rigidly maintained,25 as obstructive components are commonly involved in apparently purely central apnoeas and vice versa,39 40 as indirectly indicated in our study by the observation that in most instances, neither NIPPV nor flow-SNIPPV backup mechanical breaths produced chest wall expansion during central apnoeas.

Finally, statistically significant differences observed in the measured cardiorespiratory parameters according to the non-parametric test were lost on post hoc testing of paired groups, indicating that a larger sample size is needed to correctly interpret these results.

CONCLUSIONS
Although not conclusive, our study seems to indicate that flow-SNIPPV helps preterm infants in reducing the overall incidence of desaturation and/or bradycardia events and the incidence of central apnoea episodes. Our results, however, need to be validated with a larger number of observations and in infants treated for longer periods.

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Contributors CG had primary responsibility for protocol development, patient screening, enrolment, monitoring data collection for the whole trial, outcome assessment, preliminary and final data analysis and writing the manuscript. She is guarantor. FM participated in the development of the protocol and analytical framework for the study. He performed the analysis and elaboration of recorded signals from monitoring devices involved in the study and contributed to the drafting of the manuscript. VP participated in the development of the protocol, wrote the statistical analysis plan, monitored data collection for the whole trial and contributed to the drafting of the manuscript. CC, CMa and MC contributed to patient screening and enrolment, supervised and cared for the infants during recordings and monitored data collection for the whole trial. They also contributed to the drafting of the manuscript. PP participated in the development of the protocol providing critical input into study design, helped to perform final data analyses and assisted in drafting the manuscript. CM participated in the development of the protocol, helped to perform final data analyses and assisted in drafting the manuscript. RA supervised the design and execution of the study, performed the final data analyses and contributed to the drafting of the manuscript. All authors read and approved the final manuscript.

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Competing interests CM is a consultant to Ginevri Medical Technologies. Ginevri Medical Technologies has not contributed any financial support for this paper or had any part in the authorship.

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